



# Right entorhinal cortical thickness is associated with Mini-Mental State Examination scores from multi-country datasets using MRI

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## Abstract

**Purpose** To discover common biomarkers correlating with the Mini-Mental State Examination (MMSE) scores from multi-country MRI datasets.

**Methods** The first dataset comprised 112 subjects (49 men, 63 women; range, 46–94 years) at the National Hospital Organization Kyushu Medical Center. A second dataset comprised 300 subjects from the Alzheimer’s Disease Neuroimaging Initiative (ADNI) database (177 men, 123 women; range, 57–91 years). Three-dimensional T1-weighted MR images were collected from both datasets. In total, 14 deep gray matter volumes and 70 cortical thicknesses were obtained from MR images using FreeSurfer software. Total hippocampal volume and the ratio of hippocampus to cerebral volume were also calculated. Correlations between each variable and MMSE scores were assessed using Pearson’s correlation coefficient. Parameters with moderate correlation coefficients ( $r > 0.3$ ) from each dataset were determined as independent variables and evaluated using general linear model (GLM) analyses.

**Results** In Pearson’s correlation coefficient, total and bilateral hippocampal volumes, right amygdala volume, and right entorhinal cortex (ERC) thickness showed moderate correlation coefficients ( $r > 0.3$ ) with MMSE scores from the first dataset. The ADNI dataset showed moderate correlations with MMSE scores in more variables, including bilateral ERC thickness and hippocampal volume. GLM analysis revealed that right ERC thickness correlated significantly with MMSE score in both datasets. Cortical thicknesses of the left parahippocampal gyrus, left inferior parietal lobe, and right fusiform gyrus also significantly correlated with MMSE score in the ADNI dataset ( $p < 0.05$ ).

**Conclusion** A positive correlation between right ERC thickness and MMSE score was identified from multi-country datasets.

**Keywords** Entorhinal cortex · Mini-Mental State Examination · MRI · ADNI

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## Abbreviations

AD	Alzheimer's disease
ADNI	Alzheimer's Disease Neuroimaging Initiative
ANOVA	Analysis of variance
ASHS	Automated segmentation of hippocampal subfields
BA	Brodman area
ERC	Entorhinal cortex
GLM	General linear model
MCI	Mild cognitive impairment
MMSE	Mini-Mental State Examination
MMSE-J	Mini-Mental State Examination Japanese version
MTL	Medial temporal lobe
PHC	Parahippocampal cortex

## Introduction

Medial temporal lobe (MTL) atrophy is highly associated with cognitive performance. Neurofibrillary tangle deposition is initially seen in the transentorhinal region, while any cognitive impairments are not clinically evident at this stage [1]. The entorhinal cortex (ERC) is the key feature of Braak stage III, which is closely associated with cognitive impairment [1]. The ERC is located medial to the rhinal sulcus and comprises the anterior portion of the parahippocampal gyrus. The ERC functions as the crucial gateway between the hippocampus and neocortex [2, 3]. Thickness of the ERC is known to correlate with the effects of  $\beta$ -amyloidosis and tauopathic neurodegeneration [4, 5]. Damage to the ERC has been shown to impair cognitive function [3, 6, 7]. In addition, loss and atrophy of layer II ERC neurons are associated with memory test performance and are seen in elderly individuals preceding the onset of dementia symptoms [6].

Magnetic resonance imaging (MRI) is the most frequently utilized non-invasive technique for computing brain volume with high reproducibility. Morphological evaluation using MRI has revealed relationships between cortical thickness and cognitive test performance in healthy individuals, irrespective of scan sessions, scanners, or field strengths [8, 9].

The Mini-Mental State Examination (MMSE) is the most commonly used tool in screening for cognitive impairment. MMSE provides reliable scores without being influenced by repetition or learning, and consistent results can be obtained by the same or different examiners on repeat testing [10]. Many human studies have demonstrated that MMSE scores correlate with ERC thickness or volumes [11–18]. Long et al. found the loss of asymmetry in ERC has been shown as biomarkers to identify preclinical Alzheimer's disease (AD) [19]. Thus, right and left ERC thicknesses should have different strength of association with MMSE scores. Subfield analysis of MTL has been investigated to perform a detailed

evaluation of MTL subregions, and the analysis has offered insight into the early diagnosis and monitoring of AD [13]. However, the relevance between MMSE scores and ERC thickness in multi-country datasets remains unknown. The Alzheimer's Disease Neuroimaging Initiative (ADNI) is an open data sharing framework and the largest database of elderly subjects in the USA [20].

The present study aimed to discover common biomarkers correlating with MMSE scores using MRI datasets from both National Hospital Organization Kyushu Medical Center (KMC) and the ADNI.

## Materials and methods

### Dataset from KMC

This study was approved by the institutional review board of KMC. The requirement for informed consent for study participation was waived due to the retrospective nature of this study. Data from 200 consecutive patients (90 men, 110 women; median age, 77 years; range, 36–95 years) who underwent MRI between February 2019 and August 2020 were retrospectively analyzed. Among these, subjects who underwent testing using the Japanese version of the MMSE (MMSE-J) were included in the present study. Exclusion criteria were as follows: (i) patients with severe head motion artifacts; or (ii) patients with treatable dementias such as idiopathic normal-pressure hydrocephalus, brain tumor, metabolic, infectious, inflammatory, or drug-induced cognitive impairment, or history of stroke other than small vessel disease. Motion artifact and the presence of intracranial abnormality on the MR images were evaluated by an experienced radiologist (K.Y.).

Three-dimensional (3D) T1-weighted imaging was performed using a 1.5-T MRI unit (Magnetom Symphony Tim, Siemens, Erlangen, Germany) with a 6-channel head coil. The following scanning parameters were used: repetition time, 1700 ms; echo time, 3.4 ms; inversion time, 800 ms; flip angle, 15°; 144 sagittal sections; slice thickness =  $1.25 \times 1.25 \times 1.25$  mm<sup>3</sup>; field of view,  $230 \times 230$  mm<sup>2</sup>; matrix,  $256 \times 256$ .

### Dataset from the ADNI database

Images from 3D T1-weighted MRI were collected from the ADNI database (<http://adni.loni.usc.edu/>). The representative voxel resolution of ADNI (ADNI1) data was  $1 \times 1 \times 1.2$  mm<sup>3</sup>. The dataset comprised 300 subjects (177 men, 123 women; median age, 76 years; range, 57–91 years). These subjects comprised 100 subjects each for normal controls, mild cognitive impairment (MCI), and AD.

### Preprocessing of 3D T1-weighted images from the two datasets using the FreeSurfer pipeline

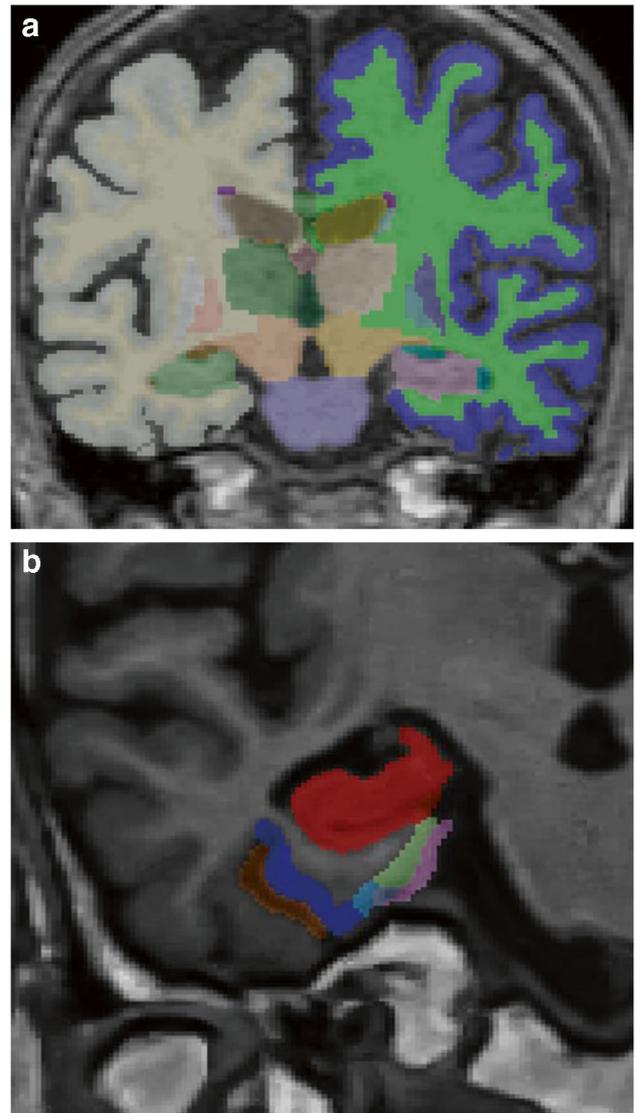
All MR images from the two datasets were preprocessed with the FreeSurfer pipeline (version 6.0.0) [21, 22], a freely available software commonly used for brain structural MRI analysis. The automatic reconstruction steps include non-uniform intensity normalization, automatic subcortical segmentation, resampling of the average curvature from the atlas to subject, cortical parcellation using the Desikan-Killiany cortical atlas [23], and parcellation statistics (<https://surfer.nmr.mgh.harvard.edu/fswiki/recon-all>). A representative parcellation image is shown in Fig. 1a. A detailed description of the reconstruction steps has been provided elsewhere [22]. The entire cortex of each subject was visually inspected, and the topological defects were manually corrected [24]. Volume data of bilateral hippocampi, amygdalas, thalami, putamina, caudate nuclei, globi pallidi, nuclei accumbentes, and total corpora callosa were collected from the cortical parcellation atlas. Mean cortical thickness of the right hemisphere, left hemisphere, and 70 cortical thicknesses (35 variables in each hemisphere) were also attained from the atlas. Total hippocampal volume and the ratio of hippocampus to the cerebral volume were also calculated. These variables including subject age were used for further analyses.

### Preprocessing of 3D T1-weighted images from the two datasets using the automatic segmentation of hippocampal subfields pipeline

All MR images from the two datasets were implemented in the automatic segmentation of hippocampal subfields (ASHS)-Penn Memory Center (PMC)-T1 pipeline (version 1.0.0) [25]. The ASHS-PMC-T1 pipeline consists of multi-atlas algorithm by manual segmentation of the MTL cortex and machine learning techniques. The detailed protocol has been reported elsewhere [13, 25]. Automated segmentation of anterior/posterior hippocampus, ERC, Brodmann areas (BA) 35 and 36, and parahippocampal cortex (PHC) from each subject via ITK-SNAP distributed segmentation service (<https://dss.itksnap.org>), and volume of each subregion was calculated using ITK-SNAP software (version 3.8.0) [26]. A representative segmentation of MTL subregions is indicated in Fig. 1b.

### MMSE

We were interested in testing whether some variables derived from multi-country datasets correlated with MMSE scores. To address this question, subjects who completed the MMSE-J at KMC or the MMSE from ADNI cohorts were included for analysis. The MMSE-J and MMSE were administered to screen for cognitive impairments, with all assessments performed by experienced examiners. MMSE-J



**Fig. 1** Representative images of the FreeSurfer automated brain parcellation (a) and the automatic segmentation of hippocampal subfields (ASHS-T1) pipeline (b).

and MMSE scores were obtained from each subject at KMC and from the ADNI database, respectively.

### Statistical analysis

All statistical analyses were performed using PASW Statistics version 18 (SPSS Inc., Chicago, IL, USA) and graphs were plotted in Prism version 7 (GraphPad Software, La Jolla, San Jose, CA, USA).

Correlations between each variable including subject age and MMSE score (MMSE-J at KMC and MMSE from ADNI cohorts) were assessed using Pearson's correlation coefficient. Overfitting occurs when too many variables included in the regression analysis [27, 28]. According

to the literatures, the parameters showing moderate correlation coefficients ( $r > 0.3$ ) [29] from each dataset were then taken as independent variables and evaluated using one-way analysis of variance (ANOVA) with general linear model (GLM) analyses. In addition, thickness of the right ERC was compared with that of the left ERC for both datasets using two-tailed Student's *t*-tests. Thicknesses of the right and left ERC were compared among normal controls, MCI, and AD from the ADNI dataset using one-way ANOVA followed by Student's *t*-tests with Bonferroni corrections for multiple comparisons, respectively.

Next, correlations between volume of each MTL subregions and MMSE score were assessed using Pearson's correlation coefficient. Parameters showing moderate correlation coefficients ( $r > 0.3$ ) from each dataset were then taken as independent variables and evaluated using GLM analysis. Volumes of right and left ERC were compared among normal controls, MCI, and AD from the ADNI dataset using one-way ANOVA followed by Student's *t*-tests with Bonferroni corrections for multiple comparisons, respectively.

Values of  $p < 0.05$  were considered indicative of statistical significance in all statistical analyses.

## Results

One hundred and twelve subjects from KMC fulfilled the criteria (49 men, 63 women; median age, 77 years; range, 46–94 years). Demographic and clinical information for subjects are presented in Table 1. Mean age did not differ significantly between datasets.

### Pearson's correlation coefficients of the dataset from KMC with the FreeSurfer pipeline

Table 2 shows the correlations between MMSE score and values from the KMC dataset. Variables with moderate

correlation coefficients ( $r > 0.3$ ) were thicknesses of the right ERC and right insular cortex, and volumes of the right amygdala and right, left, and total hippocampi. All variables with moderate correlation coefficients showed positive correlations with MMSE scores.

### Pearson's correlation coefficients of the ADNI dataset with the FreeSurfer pipeline

Table 3 shows the correlations between MMSE score and values from the ADNI dataset. More variables had moderate correlation coefficients ( $r > 0.3$ ) than KMC dataset as shown in Table 3. All variables with moderate correlation coefficients displayed positive correlations with MMSE scores.

### GLM analysis of both datasets with the FreeSurfer pipeline

GLM analysis demonstrated that right ERC thickness correlated significantly with MMSE score for the first dataset ( $p = 0.005$ ; Fig. 2a), and thickness of the right ERC ( $p = 0.039$ ; Fig. 2b), parahippocampal gyrus ( $p = 0.023$ ), left inferior parietal lobe ( $p = 0.025$ ), and right fusiform gyrus ( $p = 0.035$ ) for the ADNI dataset. Figure 2 shows scatter plots and linear regression lines for right ERC thickness from both datasets.

### Differences in right and left ERC thickness

The dataset from KMC exhibited that the right ERC tended to be thicker (mean  $\pm$  standard deviation [SD] =  $3.07 \pm 0.54$  mm) than the left ERC (mean =  $3.00 \pm 0.49$  mm), although the difference was not significant ( $p = 0.0663$ ; Fig. 3a). In the ADNI dataset, the right ERC was significantly thicker (mean =  $2.81 \pm 0.47$  mm) than the left ERC (mean =  $2.70 \pm 0.45$  mm;  $p = 0.0226$ ) (Fig. 3b).

**Table 1** Summary of demographic and clinical characteristics

Characteristic	KMC ( $n = 112$ )	ADNI		
		NC ( $n = 100$ )	MCI ( $n = 100$ )	AD ( $n = 100$ )
M/F	49/63	57/43	69/31	51/49
Age (years old)	46–94	60–90	58–89	57–91
Median age	77	76	76	75
MMSE score	9–30	25–30	24–30	18–27
Median MMSE	26	29	27	23.5

**Table 2** Pearson's *R* and ANOVA with general linear model (GLM) between KMC data and MMSE scores with the FreeSurfer pipeline

	Pearson's <i>R</i>		ANOVA with GLM
	<i>R</i> square	<i>P</i> value	<i>P</i> value
R_entorhinal	0.1682	< 0.0001	0.005*
R_hippocampus	0.1547	< 0.0001	-
Total_hippocampus	0.1423	< 0.0001	-
R_insula	0.1252	0.0001	0.050
R_amygdala	0.1188	0.0002	0.157
L_hippocampus	0.107	0.0004	-

Note: \*Statistical significance ( $p < 0.05$ ). The underscores represent volume variables

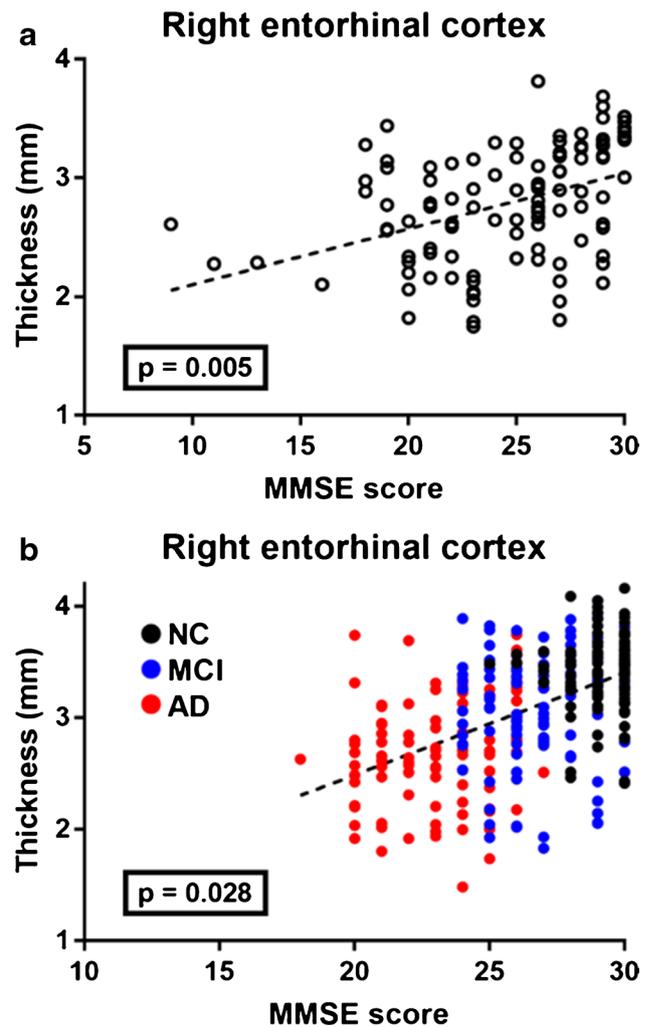
**Table 3** Pearson's *R* and ANOVA with GLM between the ADNI data and MMSE score

	Pearson's <i>R</i>		ANOVA with GLM
	<i>R</i> square	<i>P</i> value	<i>P</i> value
L_inferiortemporal	0.2741	< 0.0001	0.111
L_entorhinal	0.2535	< 0.0001	0.487
R_entorhinal	0.2487	< 0.0001	0.039*
L_middletemporal	0.2378	< 0.0001	0.189
R_fusiform	0.2361	< 0.0001	0.035*
L_fusiform	0.221	< 0.0001	0.766
Total hippocampus	0.2153	< 0.0001	0.798
L_hippocampus	0.2122	< 0.0001	0.813
<u>Hippocampus/cerebrum</u>	0.1999	< 0.0001	0.647
R_inferiortemporal	0.1951	< 0.0001	0.998
L_superiortemporal	0.1938	< 0.0001	0.322
R_middletemporal	0.1936	< 0.0001	0.444
<u>L_amygdala</u>	0.1922	< 0.0001	0.448
R_hippocampus	0.189	< 0.0001	-
L_mean cortical thickness	0.1781	< 0.0001	0.36
<u>R_amygdala</u>	0.1741	< 0.0001	0.185
R_inferiorparietal	0.1675	< 0.0001	0.492
R_mean cortical thickness	0.1593	< 0.0001	0.159
L_inferiorparietal	0.1584	< 0.0001	0.025*
L_temporalpole	0.158	< 0.0001	0.81
R_superiortemporal	0.1571	< 0.0001	0.87
L parahippocampal	0.1418	< 0.0001	0.023*
R_banks of superior temporal sulcus	0.136	< 0.0001	0.479
L_banks of superior temporal sulcus	0.1231	< 0.0001	0.677
R_temporalpole	0.1205	< 0.0001	0.503
L_precuneus	0.118	< 0.0001	0.19
L_medialorbitofrontal	0.1169	< 0.0001	0.623
R_insula	0.1098	< 0.0001	0.646
L_insula	0.1091	< 0.0001	0.256
R_precuneus	0.1067	< 0.0001	0.643
L_supramarginal	0.1055	< 0.0001	0.397
R_medialorbitofrontal	0.0994	< 0.0001	0.568
R_superiorfrontal	0.0951	< 0.0001	0.537
R_caudalmiddlefrontal	0.0938	< 0.0001	0.633
R_rostralmiddlefrontal	0.0924	< 0.0001	0.315
L_isthmuscingulate	0.0909	< 0.0001	0.675

Note: \*Statistical significance ( $p < 0.05$ ). The underscores represent volume variables

**ERC thickness among normal control, MCI, and AD**

The right ERC was thickest with normal control (mean =  $3.41 \pm 0.47$  mm), followed by MCI (mean =  $3.08 \pm 0.53$  mm) and AD (mean =  $2.73 \pm 0.50$  mm;  $p < 0.0001$ , each) in descending order (Fig. 4a). The left ERC was also the

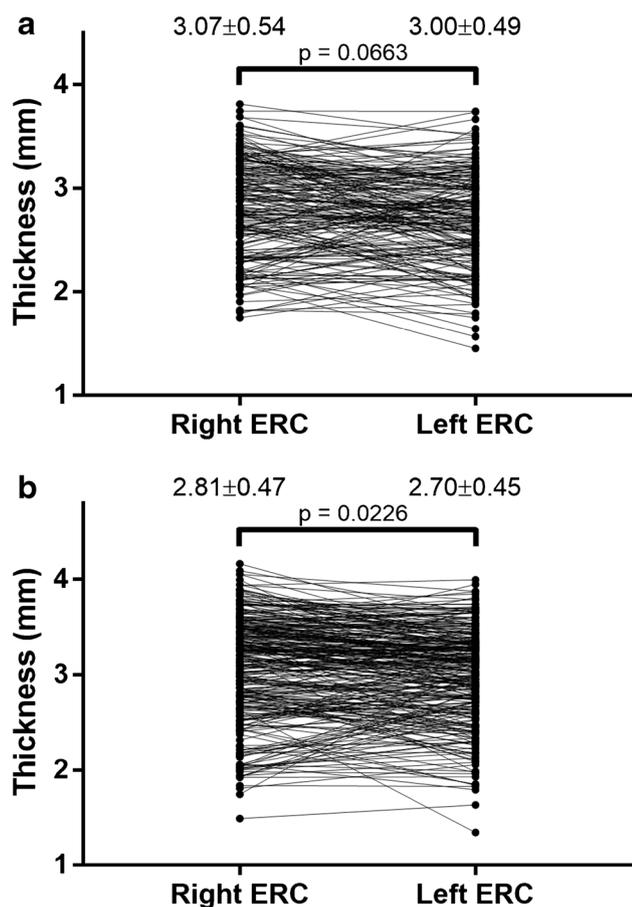


**Fig. 2** Scatter plots and linear regression lines of the right ERC thickness from National Hospital Organization Kyushu Medical Center (KMC; **a**) and the ADNI dataset (**b**). GLM analysis demonstrated that right ERC thickness correlated positively with MMSE scores for the first dataset ( $p = 0.005$ ), and thickness of the right ERC ( $p = 0.039$ ) for the ADNI dataset. NC, MCI, and AD represent normal control, mild cognitive impairment (MCI), and Alzheimer's disease, respectively.

thickest with normal control (mean =  $3.31 \pm 0.29$  mm), followed by MCI (mean =  $3.01 \pm 0.45$  mm) and AD (mean =  $2.67 \pm 0.47$  mm;  $p < 0.0001$ , each) in descending order (Fig. 4b). The right ERC was significantly thicker than the left ERC in normal control ( $p = 0.0255$ ), while we found no significant difference between them in MCI ( $p = 0.82$ ) and AD ( $p > 0.99$ ) groups.

**Pearson's correlation coefficients of the dataset from KMC with the ASHS-PMC-T1 pipeline**

Variables with moderate correlation coefficients ( $r > 0.3$ ) were volumes of the right anterior/posterior hippocampi,



**Fig. 3** Differences in the right and left ERC thickness from KMC (a) and the ADNI dataset (b). The right ERC tended to be thicker than the left ERC, although no significant difference ( $p = 0.0663$ ) was reported from KMC dataset. In the ADNI dataset, the right ERC was significantly thicker than the left ERC ( $p = 0.0226$ ).

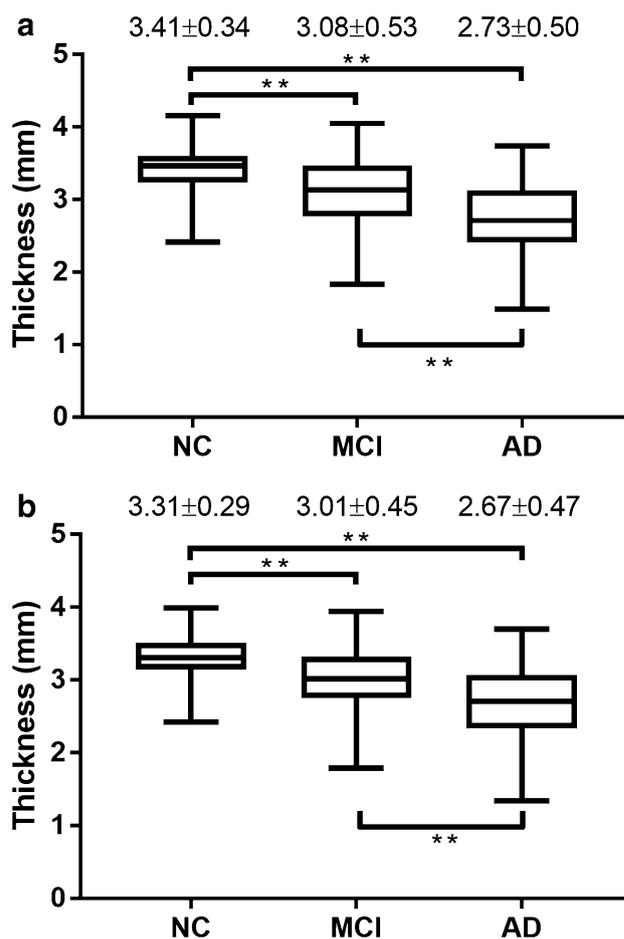
right ERC, left posterior hippocampus, and right BA35 (Table 4). All variables showed positive correlations with MMSE scores.

**Pearson’s correlation coefficients of the dataset from ADNI with the ASHS-PMC-T1 pipeline**

Variables with moderate correlation coefficients ( $r > 0.3$ ) were volumes of the right and left anterior/posterior hippocampi, right and left ERC, right and left BA35, right and left BA 36, and left PHC (Table 5). All variables displayed positive correlations with MMSE scores.

**GLM analysis of both datasets with the ASHS-PMC-T1 pipeline**

GLM analysis demonstrated that no variable correlated significantly with MMSE score for the first dataset (Table 4), while volumes of the left posterior hippocampus ( $p = 0.023$ )



**Fig. 4** Right (a) and left ERC (b) thicknesses of normal control, MCI, and AD groups. The right ERC was the thickest with normal control (mean =  $3.41 \pm 0.47$  mm), followed by MCI (mean =  $3.08 \pm 0.53$  mm) and AD (mean =  $2.73 \pm 0.50$  mm;  $p < 0.0001$ , each) in descending order (a). The left ERC was also the thickest with normal control (mean =  $3.31 \pm 0.29$  mm), followed by MCI (mean =  $3.01 \pm 0.45$  mm) and AD (mean =  $2.67 \pm 0.47$  mm;  $p < 0.0001$ , each) in descending order (b). The double asterisk indicates  $p < 0.0001$

and left BA36 ( $p = 0.012$ ; Table 5) had significant correlation with MMSE score for the ADNI dataset.

**Table 4** Pearson’s *R* and ANOVA with GLM between KMC data and MMSE scores with the ASHS-PMC-T1 pipeline

	Pearson’s <i>R</i>		ANOVA with GLM
	<i>R</i> square	<i>P</i> value	<i>P</i> value
R_posterior hippocampus	0.136	< 0.0001	0.418
R_ERC	0.1279	0.0001	0.416
L_posterior hippocampus	0.1121	0.0003	0.730
R_anterior hippocampus	0.1019	0.0006	0.598
R_BA35	0.0924	0.0011	0.841

**Table 5** Pearson's *R* and ANOVA with GLM between the ADNI data and MMSE score with the ASHS-PMC-T1 pipeline

	Pearson's <i>R</i>		ANOVA with GLM
	<i>R</i> square	<i>P</i> value	<i>P</i> value
L_posterior hippocampus	0.2217	< 0.0001	0.023*
R_posterior hippocampus	0.1727	< 0.0001	0.874
L_ERC	0.1708	< 0.0001	0.174
L_BA36	0.1445	< 0.0001	0.012*
R_ERC	0.1366	< 0.0001	0.793
L_BA35	0.1365	< 0.0001	0.541
L_anterior hippocampus	0.1363	< 0.0001	0.789
R_BA35	0.1221	< 0.0001	0.207
R_anterior hippocampus	0.1166	< 0.0001	0.666
L_PHC	0.0964	< 0.0001	0.630

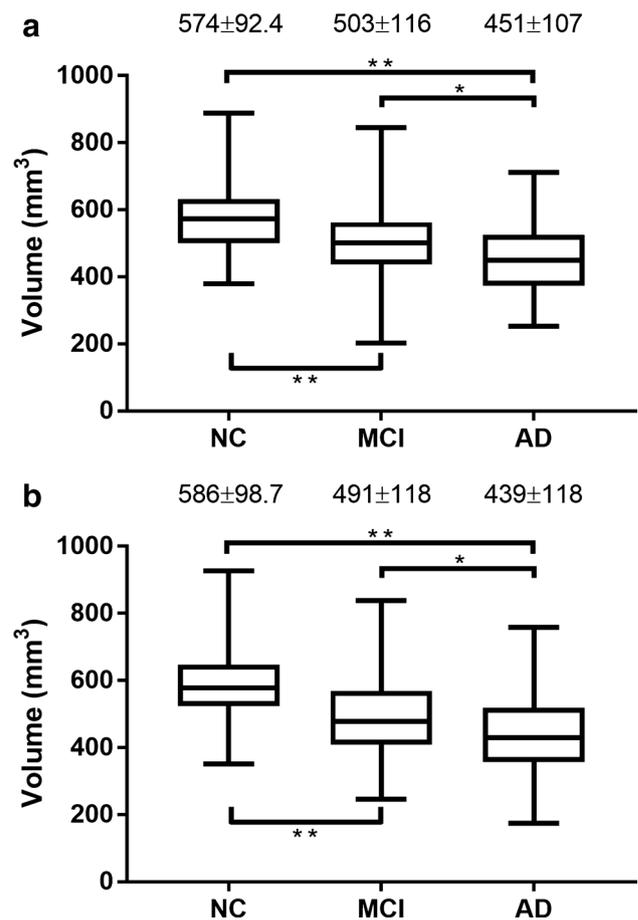
Note: \*Statistical significance ( $p < 0.05$ )

### ERC volume among normal control, MCI, and AD

The right ERC was the largest with normal control (mean =  $574 \pm 92.4 \text{ mm}^3$ ), followed by MCI (mean =  $503 \pm 116 \text{ mm}^3$ ;  $p < 0.0001$ ) and AD (mean =  $451 \pm 107 \text{ mm}^3$ ;  $p = 0.0017$ ) in descending order (Fig. 5a). The left ERC was largest with normal control (mean =  $586 \pm 98.7 \text{ mm}^3$ ), followed by MCI (mean =  $491 \pm 118 \text{ mm}^3$ ;  $p < 0.0001$ ) and AD (mean =  $439 \pm 118 \text{ mm}^3$ ;  $p = 0.0036$ ) in descending order (Fig. 5b).

### Discussion

Thickness of the right ERC was the common variable which was significantly associated with MMSE score using multi-country datasets in this study. The ERC is pivotally involved in working memory and spatial information [30–32], and mediates the interactions of memory consolidation between the hippocampus and neocortex [31]. Microscopically, grid cells are spatially modulated neurons that have been identified in and around the ERC in mammalian species [33]. Grid cells in the medial ERC generate metric spatial representations [34] and are part of a spatial coordinate system [35]. The ERC is thus the hub of a widespread brain network for navigation and spatial memory [31, 32, 35, 36]. ERC volume [19, 37] and thickness [11, 12, 14–17, 38] are reportedly associated with progression of AD. MMSE scores have been widely used to assess cognitive function. Moreover, the domain of spatial orientation and memory contributes a large proportion of potential points [39]. Taken together, ERC may play key roles in spatial orientation and memory, and MMSE scores appear reasonable to predict thickness of the ERC.



**Fig. 5** Right (a) and left ERC (b) volumes of normal control, MCI, and AD groups. The right ERC was the largest with normal control (mean =  $574 \pm 92.4 \text{ mm}^3$ ), followed by MCI (mean =  $503 \pm 116 \text{ mm}^3$ ;  $p < 0.0001$ ) and AD (mean =  $451 \pm 107 \text{ mm}^3$ ;  $p = 0.0017$ ) in descending order (a). The left ERC was largest with normal control (mean =  $586 \pm 98.7 \text{ mm}^3$ ), followed by MCI (mean =  $491 \pm 118 \text{ mm}^3$ ;  $p < 0.0001$ ) and AD (mean =  $439 \pm 118 \text{ mm}^3$ ;  $p = 0.0036$ ) in descending order (b). The single and double asterisks indicate  $p < 0.01$  and  $p < 0.0001$ , respectively.

The right ERC tended to be thicker than the left ERC in both datasets. Asymmetry of the cortical thickness reportedly correlates with cognitive function [40]. Previous research has suggested that the volume of the right ERC is greater than that of the left ERC in both normal subjects and patients with AD [37]. Volume of the right ERC was significantly associated with progression of MCI to AD [41]. The apolipoprotein E (ApoE)  $\epsilon 4$  allele is a well-established risk factor for AD [42]. Juottonen et al. suggested that the ApoE  $\epsilon 4$  allele contributes to atrophy, particularly for the right ERC [37]. That study showed an association between ApoE  $\epsilon 4$  allele and neuropathological findings such as increased amyloid plaques and neurofibrillary tangles. Interestingly, the right ERC was significantly thicker than the left ERC in normal control, while we found no significant difference

between them in MCI and AD groups. The loss of asymmetry in ERC has been shown as biomarkers to identify preclinical AD [19], and our findings are in line with the literature. These findings in our study highlighted that the difference in right ERC thickness might be more prominent than that of the left ERC, or the right ERC may play a crucial role in cognitive function.

Thicknesses of the left parahippocampal gyrus, left inferior parietal lobe, and right fusiform gyrus for the ADNI dataset significantly correlated with MMSE scores in GLM analyses from the ADNI dataset, but significantly correlated with MMSE scores only in Pearson's correlation coefficients from the dataset at KMC. It has been reported that volume of the left parahippocampal gyrus is indicative of early biomarker of AD [43]. Some genetic variations might influence the atrophy rates of parahippocampal gyrus [44]. Mental representations are processed within the inferior parietal lobule [45]. Mental representation could be influenced by racial-ethnic group differences in individualism and collectivism [46]. Right fusiform gyrus is involved in face perception, and damage to the right fusiform gyrus resulted in the impairments to normal face recognition [47]. The difference in correlations between thickness of the right fusiform gyrus and MMSE scores from the two datasets might be reduced by perceptual training for other race effects [48], but this issue is beyond scope of the present study. We also observed that volumes of the left posterior hippocampus and left BA36 had significant correlation with MMSE score from the ADNI dataset. Similar findings have been reported in patients with early stages of AD [13, 49]. BA36 has been reportedly associated with personality changes such as agreeableness and openness [50]. These personality changes might influence the discrepancy on the GLM analysis between the two datasets in our study.

In Pearson's correlation coefficients, more variables including hippocampus volume were associated with MMSE scores in our study. A plethora of evidence has suggested that hippocampus volume is closely related to cognitive function. Our results provide informative data to help discern the correlations between volume of the hippocampus and MMSE scores in a non-invasive manner.

To obtain common characteristics from multi-country datasets, the preprocessing pipeline needs to be taken into consideration regarding morphological differences between various races and ethnicities across multi-country datasets. The FreeSurfer pipeline has been used worldwide to acquire quantitative variables in the brain [22]. Discovery of a common variable from multi-country datasets appears reasonable for understanding how MMSE scores are influenced by the thickness of the right ERC. In summary, the present study may allow non-invasive creation of predictive models in multi-country datasets non-invasively.

Our study has several limitations. First, handedness data was unavailable and thus might have influenced the laterality result. However, the volume of the right ERC is reportedly larger than left ERC volume in both normal subjects and patients with AD [37]. This study did not take into account the potential for differences in the questionnaire or detailed rating scales between MMSE and MMSE-J. Lastly, MR images were acquired on a 1.5-T unit in the present study. Xie et al. proposed the ASHS-PMC-T1 pipeline without T2-weighted images [13] although the combination of T1- and coronal T2-weighted images using a 3.0-T unit may provide better segmentation results when analyzing MTL subfield.

In conclusion, we found the positive correlations between right ERC thickness and MMSE scores using multi-country datasets. Computing right ERC thickness may be a potential option in patients with cognitive impairment without regard to race or ethnicity.

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## Declarations

**Conflict of interest** The authors declare that they have no conflict of interest.

**Ethical approval** This retrospective study was approved by National Hospital Organization Kyushu Medical Center Institutional Review Board for Clinical Research.

**Informed consent** Informed consent was waived because this study was retrospective nature.

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